



Resolving the Effect of Phase Errors on Ultrafast Ultrasound Plane Wave Imaging

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ABSTRACT

The phase error caused by non-ideal physical transducer characteristics can affect the ultrasonic wave front during beamforming. If not compensated, the phase error can degrade the focusing capability and reduce the B-mode image spatial resolution. In this paper, the effect of the phase error on ultrafast coherent plane wave imaging (CPWI) was investigated using a bespoke ultrasound imaging system, ultrasound array research platform II (UARP II). The phase deviations between the aligned radio frequency (RF) signals from all active elements were calculated by applying cross-correlation techniques with the RF signal from the first active element as the registration reference. A sign-reversed lag technique has been applied to the RF signals to encounter the phase error. When the phase error was corrected, the lateral resolution at -6 dB and -20 dB showed improvements from 0.42 mm to 0.34 mm and from 1.18 mm to 0.56 mm, respectively. No significant changes occurred for the axial main lobe.

1. INTRODUCTION

The phase error is a terminology used to describe the deviation between the aligned radio frequency (RF) echo from each element during ultrasound beamforming. This happens mainly due to two reasons. Firstly, it is because of the non-ideal physical transducer characteristics and the second reason is the non-uniform speed of sound in the imaging medium [1-2]. The characteristics of each transducer are defined by a fixed central frequency, limited bandwidth, damping and sensitivity. Each transducer element is unique and none of them are same [3-4]. At the same time, not all elements in a transducer respond or vibrate equally and there is a deviation in between of them [1].

In an ideal case, it is expected the calculated time delays added to the received RF signals will align those signals before coherent summation [5-10]. However, in a real scenario the aligned RF signals are not always in phase due

to the above reasons [11-13]. Many techniques have been proposed to estimate the phase error in ultrasound B-mode imaging. Some of the estimation techniques are the speckle brightness method [1] and the autocorrelation technique [14].

In this paper, only the phase error caused by the non-ideal physical transducer characteristics will be considered and compensated. But the proposed solutions, adding a sign-reversed lag to the RF signals can be applied to the correction of phase errors caused by the varied speed of sound as well.

2. MATERIAL AND METHOD

2.1 Experimental Setup

In order to analyse the effect of the phase error on plane wave imaging (PWI), a study was conducted on the wire targets located inside the degassed and deionized water as shown in Figure 1.

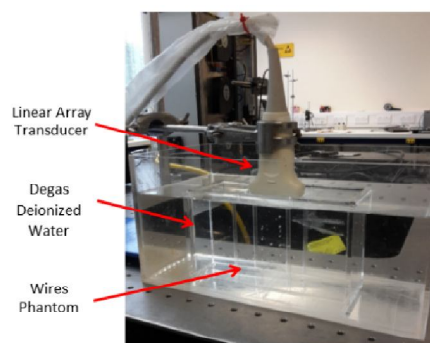


Figure 1: Experimental setup to scan wires phantom inside degassed and deionized water.

Performing ultrasound imaging in water is an advantage since the medium attenuation is very low and no other scattering except that from the wire point targets. The experiments were conducted with the parameters shown in Table 1.

Table 1: Experimental Parameters

Properties	Values
Speed of Sound in Water, m/s	1482
Attenuation Water, dB/MHz/cm	0.002
Number of Elements	128
Transducer Centre Frequency, MHz	4.79
-6 dB Transducer Bandwidth, %	57
Transducer Element Pitch, mm	0.3048
Sampling Frequency, Tx/Rx, MHz	160/80
Excitation Signal	2-cycle Sinusoid

2.2 Ultrasound Array Research Platform II (UARP II)

The UARP II is a custom ultrasound imaging system developed by the Ultrasonics and Instrumentation Group at the University of Leeds [3,4,15,16,17,18]. It contains an 8-field programmable gate array (FPGA) backplane which connects a computer running any 64-bit version of the Windows operating system (OS) via a peripheral component interconnect express (PCIe) link. Each FPGA card consists of 16 channels and there are total of 128 channels in the current UARP II. However, the design of this system is highly flexible, and the system can be easily scaled to have more channels. All excitation signals except the square pulse are designed in the Matlab software (The MathWorks Inc., Natick, MA, USA) by using a harmonic reduction pulse width modulation (HRPWM) method [15]. The sampling rate for Tx is 160 MHz. Those signals are then uploaded to the UARP II which excites the connected probe by using a five-level switched mode excitation scheme [3]. The received radio frequency (RF) data are acquired at an 80-MHz sampling rate and processed off line using MATLAB. The maximum sampling depth for a single firing can be more than 32768 samples per channel, which equates to a round trip in water of approximately 61 cm with the speed of sound of 1482 m/s at 22° C.

2.3 Beamforming

The wire targets were imaged with PWI and beamformed with the delay-and-sum (DAS) technique. The B-mode image was log-compressed and displayed with a dynamic range of 50 dB. The B-mode image was formed point by point, (x_f, z_f) with different sets of time delays assigned to the same received RF signals according to equation [19]:

$$\tau_i(x_f, z_f) = \frac{z_f \cos(\theta_n) + x_f \sin(\theta_n) + \frac{L}{2} \sin(\theta_n)}{c} + \frac{\sqrt{z_f^2 + (x_i - x_f)^2}}{c} \quad (1)$$

where $i=1, 2, 3\dots 128$, L is the aperture, θ_n is the steering angle and n is steered plane waves. In this study a single plane wave was employed, and thus, $\theta_n = 0^\circ$ and $n = 1$. The

computed time delays were added to the received RF signal $s_i(t)$, giving the aligned RF signal $v_i(t)$, which can be represented by the following equation [20]:

$$v_i(t) = s_i(t - \tau_i(x_f, z_f)) \quad (2)$$

The phase deviation between the aligned RF signals, $v_i(t)$ on all the elements were calculated by applying cross-correlation techniques relative to the RF signals from element 1, $v_1(t)$ according to the following equation:

$$p_{vvi}(\tau) = \sum_{t=t_1}^{t_2} v_1(t)v_i(t + \tau) \quad (3)$$

Where $t_1=40 \mu\text{s}$, $t_2=43.75 \mu\text{s}$. The time duration equivalent to the total number of 300 or 6000 samples for the sampling frequencies of 80 MHz and 1600 MHz respectively. The time period selected as the wire targets located at the 20 mm depth.

The lag value between the $p_{vvi}(\tau)$ signal peaks to the origin of the signal, $p_{vvi}(\tau = 0)$ determine the phase deviation between the RF signals.

3. RESULTS

The aligned RF signals for the imaging line located at $x_f=0.5 \text{ mm}$ as shown in Figure 2 for the wire target at the 20 mm depth have been used to analyze the effect of phase errors.

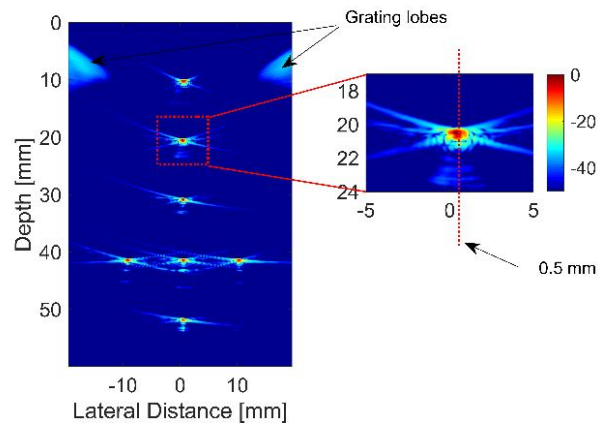


Figure 2: B-mode image of point targets beamformed with DAS obtained with PWI. The red dashed line marked on the point target at 20 mm depth shows the imaging line chosen for phase error analysis.

In an ideal case, aligning the RF signals for the central imaging line, for a wire target located at the center of the imaging medium, is expected to produce a set of RF signals in a straight-line form parallel to the face of the transducer. Thus, any deviation in the aligned RF signals can be considered as the result of phase error. A portion of the aligned RF signals obtained for the wire target at the 20 mm depth is shown in Figure 3(a). It can be seen that the signals

were not perfectly straight (aligned) and still maintained the parabolic shape of the Rx echo signal. Figure 3(b) shows the RF signals from the elements 1, 64 and 128. Qualitatively, all of the RF signals on those elements were not in-phase with each other. The RF signals between elements 1 and 64 have a phase shift of approximately 76° and 38° between elements 1 and 128.

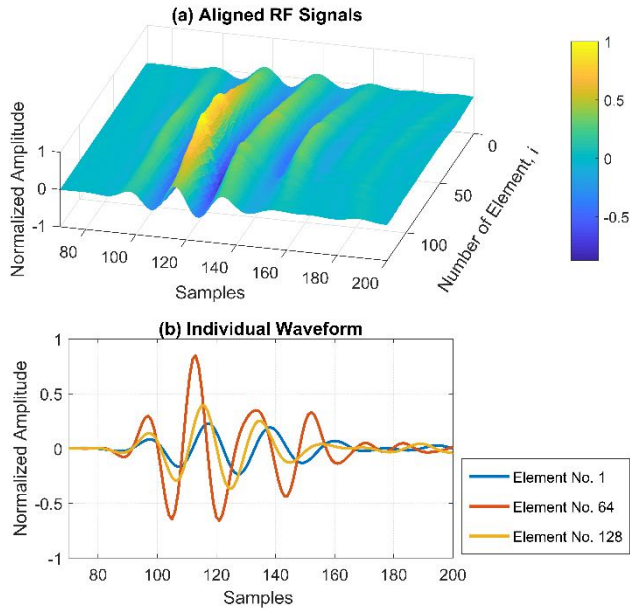


Figure 3: a) Aligned RF signals for the imaging line at $x_f=0.5$ mm at the 20 mm depth and b) individual waveforms from elements 1, 64 and 128.

The phase error was computed with two different sampling frequencies. The first is the UARP II hardware Rx sampling frequency of 80 MHz and the second is a higher sampling frequency of 1600 MHz produced by up-sampling the time domain signal $v_i(t)$, using the linear interpolation technique. The results obtained with the higher sampling frequency provided more details on the phase error compared to that with the lower sampling frequency. The accurate estimated phase error helps to determine more precisely the number of samples needed to align the RF signals. The result is shown in Figure 4.

The maximum and total phase errors for a single imaging line calculated for 128 elements with the sampling frequencies of 80 MHz and 1600 MHz are given in Table 2. The higher sampling frequency provides more accurate results than the lower sampling frequency. The time calculated with a higher frequency shows an increase of 6.26 % from 50 ns to 53.13 ns, while the distance shows an increase of 6.4 % from 37 μm to 39.37 μm . This is because the interpolation function can increase the accuracy by adding the missing data [21-25].

Once the phase error represented by the lag values was calculated, a sign-reversed lag value was applied to the aligned RF signals in order to compensate for the aberration. Figure 5 shows the results before and after phase correction takes place on the wire target at 20 mm depth.

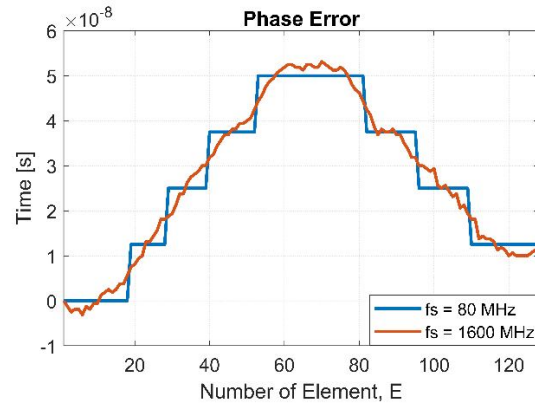


Figure 4: Phase errors measured on the aligned RF signals relative to the first element for the imaging line at $x_f=0.5$ mm in the lateral direction as shown in Figure 2.

Table 2: Phase Error

	80 MHz		1600 MHz	
	Time, ns	Distance, μm	Time, ns	Distance, μm
Maximum Phase Error	50	37	53.13	39.37
Total Phase Error	3450	3560	3462.5	2565.7

Two different regions, A and B have been chosen on the B-mode image to highlight the noise pattern changes according to the sampling rate. In region A, more side lobes and clutter noise are produced on both sides of the wire target when the lower sampling rate, 80 MHz was used to correct the phase error. This means the compensated RF signals are still not properly aligned. Correcting the phase aberration with both low and high sampling frequencies can reduce noise in the lateral direction. This has been highlighted in region B in Figure 5.

As shown in Figure 6, the main lobe in the lateral direction has been improved when the aligned RF signals are compensated with both lower and higher frequencies. The lateral resolution at -6 dB and -20 dB showed improvements from 0.42 mm to 0.34 mm and from 1.18 mm to 0.56 mm, respectively. No significant changes occurred on the axial main lobe. However, the peak side lobes (PSLs) have increased from -30 dB to -20 dB after the correction. The small amount of the increment (from -26 dB to -24 dB) in PSL can be also seen in the axial direction.

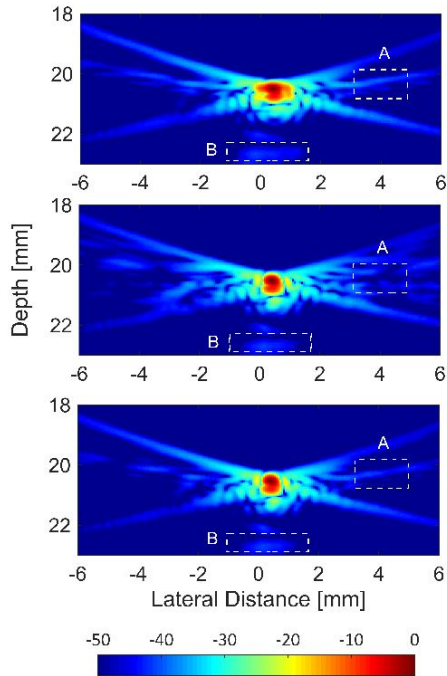


Figure 5: B-mode image of the wire target at 20 mm depth with phase error (Top), after phase error correction with the sampling rate of 80 MHz (Middle) and after phase error correction with the sampling rate of 1600 MHz (Bottom). The dashed boxes, marked with A and B, show the effect of phase correction on noisy regions.

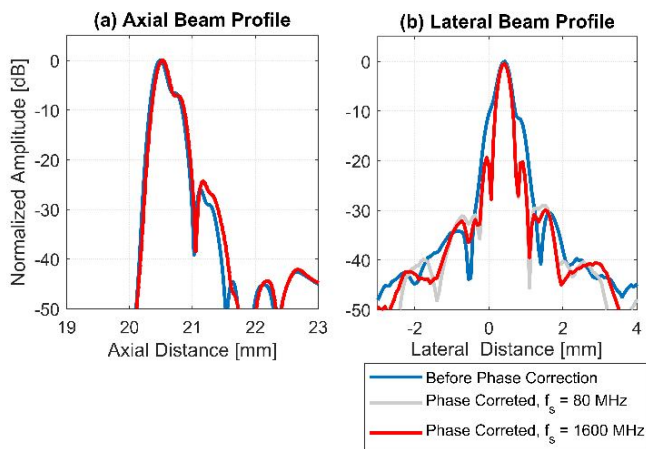


Figure 6: Beam profiles of the wire target at 20 mm depth in the a) axial direction and b) lateral direction before and after correction of phase errors.

4. CONCLUSION

The phase error that occurs due to the non-ideal transducer characteristic can be overcome by adding a sign-reversed lag to the aligned RF signals. Higher sampling rate signals are able to produce the same lateral resolution as low sampling signals. However, noise that is present on the B-mode image is much less with a higher sampling rate. The phase

corrected signal can improve the signal resolution in the lateral direction and reduce the noise level. On the other hand, the side lobes are not eliminated and are still visible within the imaging region.

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